Leukaemia Identification based on Texture Analysis of Microscopic Peripheral Blood Images using Feed-Forward Neural Network

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ABSTRACT

Leukaemia is very dangerous because it includes liquid tumour that it cannot be seen physically and is difficult to detect. Alternative detection of Leukaemia using microscopy can be processed using a computing system. Leukemia disease can be detected by microscopic examination. Microscopic test results can be processed using machine learning for classification systems. The classification system can be obtained using Feed-Forward Neural Network. Extreme Learning Machine (ELM) is a neural network that has a feedforward structure with a single hidden layer. ELM chooses the input weight and hidden neuron bias at random to minimize training time based on the Moore Penrose Pseudoinverse theory. The classification of Leukaemia is based on microscopic peripheral blood images using ELM. The classification stages consist of pre-processing, feature extraction using GLRLM, and classification using ELM. This system is used to classify Leukaemia into three classes, that is acute lymphoblastic Leukaemia, chronic lymphoblastic Leukaemia, and not Leukaemia. The best results were obtained in ten hidden nodes with an accuracy of 100%, a precision of 100%, a withdrawal of 100%.

Keywords: Leukaemia, Feature Extraction, Classification, Microscopic Peripheral Blood, Texture Analysis, Feed-Forward Neural Network.

1. INTRODUCTION

Leukaemia and Lymphoma Society states that Leukaemia is a deadly disease for all ages [1]. Leukemia is a blood disorder in the bone marrow that attacks blood-forming cells [2]. Leukemia is in the form of a liquid tumor so that it cannot be seen physically and is difficult to detect [3]. If the bone marrow produces excessive or abnormal white blood cells, it can affect the white blood cells to protect the body, which is usually called leukaemia. Leukaemia, based on its length of time, is classified into acute leukaemia and chronic leukaemia [4].

World Health Organization (WHO) states that there are approximately 150,000 people with leukaemia of acute lymphocytic type in each year with a relatively high mortality rate in Indonesia [5]. However, early detection is difficult because the general symptoms of leukaemia are not quickly recognised [6]. Alternative detection of Leukaemia using microscopy can be processed using a computing system. Leukemia disease can be detected by microscopic examination [7]. Microscopic examination counts the number of blood cells in the body. The computing process in the leukaemia diagnosis system is carried out by a classification process based on the results of microscopic examinations [8].
Previously, several studies have been conducted regarding the classification of Leukaemia. Rangole used neural networks for Leukaemia detection and obtained the best results with an accuracy of 83.33% [9]. Jyoti Rawat also implemented another method to detect leukaemia, that is feature extraction using the Gray-Level Co-Occurrence Matrix (GLCM) which obtained the best results with an accuracy of 89.8% [10]. Sendren proved that the performance of the Gray-Level Run Length Matrix (GLRLM) was better than the GLCM method [9]. The difference between GLCM and GLRLM was found in the matrix and statistical characteristics obtained. These statistical characteristics would be used as input in classifications using machine learning [12], [13].

In recent years, there have been developments of machine learning, one of which is an Feed-Forward Neural Network. Extreme Learning Machine (ELM) is a neural network that has a feedforward structure with a single hidden layer [14]. ELM is widely used to complete classification. Nemissi uses ELM for the classification of breast cancer with excellent results. Besides, ELM has also been used to solve problems such as forecasting the inflation rate in Indonesia [14], the detection of dengue fever [15], the diagnosis of breast cancer [16], and others showing results with an average accuracy rate above 90%. Gowthaman compares SVM with ELM. From several experiments, it is concluded that ELM is better than SVM in terms of results and learning speed [15].

2. MATERIAL AND METHODS

The classification system used microscopic peripheral blood image data to identify leukemia into three classes: acute, chronic, and non-leukemia, using the ELM method. Microscopic peripheral blood images were obtained from the Acute Lymphoblastic Leukaemia Image Database for Image Processing (ALL-IDB). This dataset consisted of 161 microscopic peripheral blood images with 49 Acute Lymphoblastic Leukaemia blood image data, 53 chronic lymphoblastic Leukaemia image data, and 59 non-leukaemia blood image data [18]. There are three stages in this system: pre-processing, feature extraction, and classification.

The Pre-processing stage is used to improve image quality before the feature is taken. Microscopic peripheral blood data is an RGB image. Next, RGB images are converted into grayscale images before the feature extraction process. The next step is histogram equalization to correct the intensity because the image has an uneven intensity. Then, the filtering process uses a median filter. The purpose of filtering is to eliminate noise contained in the image. After improving image quality, the next process is feature extraction using GLRLM to obtain the features contained in the image.

The first step in feature extraction using GLRLM is to construct a run-length matrix using \( p(r, t | \theta) \) where \( r \) is the grey level, \( t \) is the number of occurrences of run length, and \( \theta \) is the direction of direction orientation. These features are used as input for the classification process.

The next stage is the division of data into two, that is training data and testing data. Data sharing uses the k-fold cross-validation. Training data is intended for the learning process of classification systems. Testing data is intended for testing the results of the classification. This learning process uses ELM. The input matrix in ELM is processed with weights and biases that have been initialized in advance to obtain the output of the hidden layer. The activation function is used to obtain the output of the hidden layer.
layer. The hidden layer output is an H matrix obtained from Equation 10. Then, the pseudo-inverse model is calculated. The pseudo-inverse model is used to calculate the value of beta weights ($\beta$) using equation 13. After obtaining $\beta$, the next process is training. The training is conducted using testing data with the same weight and bias values as the learning process. After that, the $H$ matrix from the testing data is calculated. The $H$ matrix is multiplied by $\beta$ to obtain the classification results. The illustration of research step is shown in flowchart Figure 1.

![Flowchart](image)

**FIGURE 1. Research Flowchart**

### 2.1 GRAY LEVEL RUN-LENGTH MATRIX

Gray-Level Run Length Matrix is one of the methods used to extract features contained in an image to obtain statistical functions or features included in the model by estimating pixels with the same degree of gray [19]. If it is known that the run-length matrix with the matrix element $p(r, t | \theta)$ gives the total number of occurrences of run that has length $t$ of gray-level $r$ in a given direction orientation $\theta$ [20]. The direction orientation is formed with four shift directions and Galloway said that several types of statistical features could be extracted from the run-length matrix, that is[21]:

#### 2.1.1 SHORT RUNS EMPHASIS (SRE)

Short Runs Emphasis (SRE) is a feature of measuring the distribution of short runs in the image. SRE is small if the image has a smooth texture, while large SRE means that the image has a rough surface [22].

$$SRE = \frac{\sum_{r=1}^{K} \sum_{t=1}^{L} \frac{p(r,t|\theta)}{t^2}}{\sum_{r=1}^{K} \sum_{t=1}^{L} p(r,t|\theta)}$$

(1)

**Description:**

- $p(r,t|\theta)$: The run-length matrix
- $r$: Grey level of image
2.1.2 **LONG RUNS EMPHASIS (LRE)**

Long Runs Emphasis (LRE) is a feature of measuring the long-run distribution in the image. LRE is large if the texture is smooth but small LRE means rough surface [9s].

\[ LRE = \sum_{t=1}^{L} \sum_{r=1}^{K} t^2 p(r, t|\theta) / \sum_{t=1}^{L} \sum_{r=1}^{K} p(r, t|\theta) \]  

(2)

2.1.3 **GRAY LEVEL NON-UNIFORMITY (GLN)**

Gray Level Non-uniformity (GLN) is a feature that shows the degree of gray in all parts of the image. The smaller the GLN value, the more evenly the level of gray in an image.

\[ GLN = \sum_{r=1}^{K} (\sum_{t=1}^{L} p(r, t|\theta))^2 / \sum_{t=1}^{L} \sum_{r=1}^{K} p(r, t|\theta) \]  

(3)

2.1.4 **RUN LENGTH NON-UNIFORMITY (RLN)**

Run Length Non-uniformity (RLN) measures the run-length equation throughout the image. RLN is small if the run length is the same as the whole image.

\[ RLN = \sum_{t=1}^{L} (\sum_{r=1}^{K} p(r, t|\theta))^2 / \sum_{t=1}^{L} \sum_{r=1}^{K} p(r, t|\theta) \]  

(4)

2.1.5 **RUN PERCENTAGE (RP)**

Run Percentage (RP) measures the uniformity and distribution of the run of an image in a particular direction. RP is large if the run length is 1 for all gray levels for a specific direction.

\[ RP = \frac{1}{N} \sum_{r=1}^{K} \sum_{t=1}^{L} p(r, t|\theta) \]  

(5)

2.2 **EXTREME LEARNING MACHINE (ELM)**

Extreme Learning Machine (ELM) is part of a feedforward artificial neural network, which is also known as Single Hidden Layer Forward Feed Neural Networks [24]. In conventional artificial neural networks, updating the input weights and hidden neurons requires a complex computational process with a long enough time for iterations to optimize the weights [25]. ELM chooses the input weight and hidden neuron bias at random to minimize training time based on the Moore Penrose Pseudoinverse theory. In this way, ELM can work in complex datasets and with minimal time [26].
2.2.1 INITIALIZE

Initialize $a$, $f(u)$, $w$ and $b$. There are $N$ samples $(a_i, y_i)$ with $a_i = [a_{i1}, a_{i2}, ..., a_{in}]' \in \mathbb{R}_n$ and $y_i = [y_{i1}, y_{i2}, ..., y_{in}]' \in \mathbb{R}_n$. $n = \text{number of parameters}$ and with $m$ hidden neurons and the activation function $f(u)$. Where $w_{ij} = [w_{11}, w_{22}, ..., w_{nm}]'$ is a weight vector that connects nodes in the hidden layer to $w$ nodes from the input layer and $b$ is a bias weight [27].

2.2.2 CALCULATE HIDDEN LAYER OUTPUT (H)

$$H = \begin{bmatrix} f(a_{1,1}w_{11} + b_1) & \cdots & f(a_{1,m}w_{1m} + b_m) \\ \vdots & \ddots & \vdots \\ f(a_{N,1}w_{N1} + b_1) & \cdots & f(a_{N,m}w_{Nm} + b_m) \end{bmatrix}$$ (6)

2.2.3 CALCULATE WEIGHT OUTPUT

$$\beta = H^\top T$$ (7)

Description:
- $f(u)$: Activation function
- $w_j$: Weight vector that connects nodes on the hidden layer to $w$ with nodes from the input layer
- $y_i$: Label of images
- $N$: Number of data inputs
- $n$: Number of parameters
- $m$: Number of hidden layers
3. RESULT AND DISCUSSION

In this study, the Leukaemia classification system was designed using Extreme Learning Machine based on microscopic peripheral blood images. The following data samples from various levels of lymphoblastic Leukaemia are shown in Figure 3. There are three stages in this system: pre-processing, feature extraction, and classification.

(a) Normal Blood.

(b) Acute Lymphoblastic Leukaemia.

(c) Chronic Lymphoblastic Leukaemia.

FIGURE 3. Samples of Microscopic Peripheral Blood Images

The microscopic peripheral blood image is used as an input in the Leukaemia classification system using the Extreme Learning Machine. The stages of this research consist of pre-processing, feature extraction, and classification. The first stage is pre-processing. The microscopic peripheral blood image is changed to grayscale. The grayscale process aims to take grayscale images so that it can facilitate the pre-processing. In the preprocessing stage, it is applied histogram equalization process to enhancing the light intensity of the image.

The histogram equalization process is then performed. The purpose of histogram equalization is to level the light intensity of the image. The reason for the existence of a histogram equalization process is because the data processed has varying light intensities. The next process is median filter. A median filter is used to remove noise
contained in the image. The improved quality images are used as input in the feature extraction process. The following is the after pre-processing image samples shown in Figure 4.

(a) Input Image  
(b) Image After Grayscale

(c) Image After Histogram Equalization  
(d) Image After Median Filter

FIGURE 4. Pre-processing Result

The first step of feature extraction using GLRLM is to create a run-length matrix. From the matrix, several features will be obtained, including SRE, LRE, GLN, RLN and RP. In this study, a run-length matrix was formed from each direction orientation of $0^\circ$. The following feature samples from six images of the $0^\circ$ orientation are presented in Table 1.

Based on Table 1, it is shown that the LRE value of non-leukaemia blood image is greater than that of the ALL patient’s blood image and the ALL patient’s blood image has a higher LRE value than the CLL patient’s blood image. The most significant LRE value obtained is the non-leukaemia blood image which means that this image has a rough texture. This corresponds to a small SRE. While the LRE value of CLL patient images has the least value, which is around 2.06. It means that the CLL patient’s blood images have smooth textures. This is because the number of the long run is small.

<table>
<thead>
<tr>
<th>Image</th>
<th>SRE</th>
<th>LRE</th>
<th>GLN</th>
<th>RLN</th>
<th>RP</th>
<th>Class</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>0.550</td>
<td>9.417</td>
<td>658321.805</td>
<td>67025.136</td>
<td>3.335</td>
<td>Normal</td>
</tr>
<tr>
<td>2</td>
<td>0.544</td>
<td>9.991</td>
<td>638747.423</td>
<td>69185.604</td>
<td>3.291</td>
<td>Normal</td>
</tr>
<tr>
<td>3</td>
<td>0.634</td>
<td>7.653</td>
<td>437172.782</td>
<td>27380.224</td>
<td>2.658</td>
<td>ALL</td>
</tr>
<tr>
<td>4</td>
<td>0.625</td>
<td>7.936</td>
<td>417708.780</td>
<td>28055.258</td>
<td>2.609</td>
<td>ALL</td>
</tr>
<tr>
<td>5</td>
<td>0.865</td>
<td>2.068</td>
<td>813890.113</td>
<td>19528.020</td>
<td>3.256</td>
<td>CLL</td>
</tr>
<tr>
<td>6</td>
<td>0.857</td>
<td>2.100</td>
<td>774658.421</td>
<td>19817.787</td>
<td>3.222</td>
<td>CLL</td>
</tr>
</tbody>
</table>

TABLE 1.
Result of Feature Extraction Samples Using GLRLM
The next step is classification. ELM is used for the classification process of the data obtained from the previous image processing. The classification process consists of two stages, that is training stage and testing stage. The training stage is to build the best model while the testing stage is to test the accuracy of the model formed. This study used 128 data for the training stage and 33 data for the testing stage. The training and testing conducted used the ELM classification method. In this study, Leukaemia classification used five parameters obtained from the feature extraction using GLRLM, that is SRE, LRE, RLN, GLN, and RP grouped into three classes, that is non-leukaemia (normal), Acute Lymphoblastic Leukaemia (ALL) and Chronic Lymphoblastic Leukaemia (CLL). The value of the features obtained has a different range so that the normalization process is required to facilitate the training stage and the testing stage. The training stage is done by finding the H matrix using random weights and biases. Next, the output weight ($\beta$) is calculated. The output weight of the training process is called optimal beta. Then, the network output based on testing data using the optimal beta is calculated. The output is validated using several criteria, that is accuracy, precision, and recall. The following is the results of Leukaemia classification using ELM shown in Table 2 and visualize in Figure 5.

**TABLE 2.**

<table>
<thead>
<tr>
<th>Angle of GLRLM</th>
<th>Hidden Nodes</th>
<th>Accuracy</th>
<th>Precision</th>
<th>Recall</th>
<th>Average Accuracy</th>
</tr>
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<td>0</td>
<td>10</td>
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<td>15</td>
<td>96.88</td>
<td>96.97</td>
<td>96.67</td>
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<td>96.97</td>
<td>97.44</td>
<td>96.67</td>
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<td>97.44</td>
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</tbody>
</table>
Table 2 shows the evaluation results of corner trials on GLRLM and hidden nodes on EL. At the GLRLM angle of 0 degrees, the highest accuracy reaches 100% accuracy with the number of hidden nodes 10 and 13. The number of hidden nodes 13 reaches the highest accuracy of 100% at each angle. The GLRLM implementation with angles of 45, 90, and 135 degrees and the number of hidden nodes 12, 14, and 10 also has a perfect system performance with accuracy reaching 100%. The average system evaluation results at each angle are visualized in Figure 5.

**FIGURE 5. Classification Result Using ELM**

Based on Figure 4, the average accuracy results at each angle indicate that the feature extraction results using the GLRLM method can represent microscopic peripheral blood images well. The best average accuracy, precision, and recall results from all trials were obtained using the 45-degree angle GLRLM method. The average value of each accuracy, precision, and recall at an angle of 45 degrees is 98.36%, 98.50%, and 98.31%. The second order of classification systems is based on the value of accuracy, namely by using an angle of 0 degrees which is 0.43% lower than the average accuracy at an angle of 45. While the lowest result is a classification system using image features produced by the GLRLM method at an angle of 90 degrees with the average value of each -accuracy, precision, and recall are 97.41%, 97.62%, and 97.37%.

4. CONCLUSION

The Leukaemia classification model using extreme learning machine based on GLRLM features with 161 microscopic peripheral blood data showed good performance. The results of Leukaemia classification into three classes, that is non-leukaemia, ALL and CLL obtained the best results using 0° orientation with the number of neurons in the hidden layer as much as 10 with an accuracy of 100%, a precision of 100% and a recall of 100%. This model had a fast calculation time of 0.2 seconds. This showed that the extreme learning machine could classify the data with an excellent performance and fast time. Additional data was required to generate a better model.
REFERENCES


